

EDMI Microsystems and Microelectronics

MICRO-614: Electrochemical Nano-Bio-Sensing and Bio/CMOS interfaces

Lecture #15 Portable, Implantable, and Wearable Devices,...& Beyond!!!

Glucometer on iPhone



Wearable Glucometer by Abbot

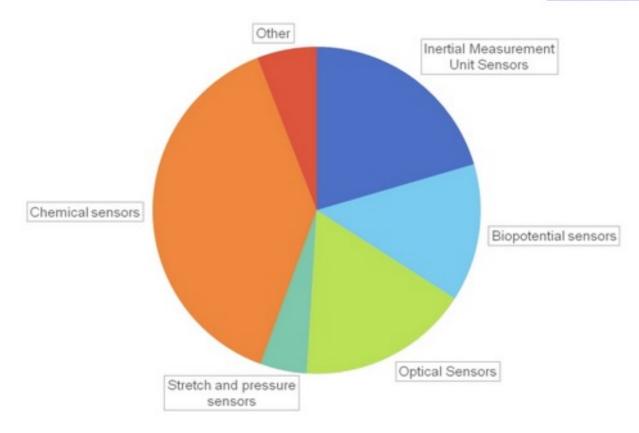


An Unser's interface

Wearable Devices by 2025

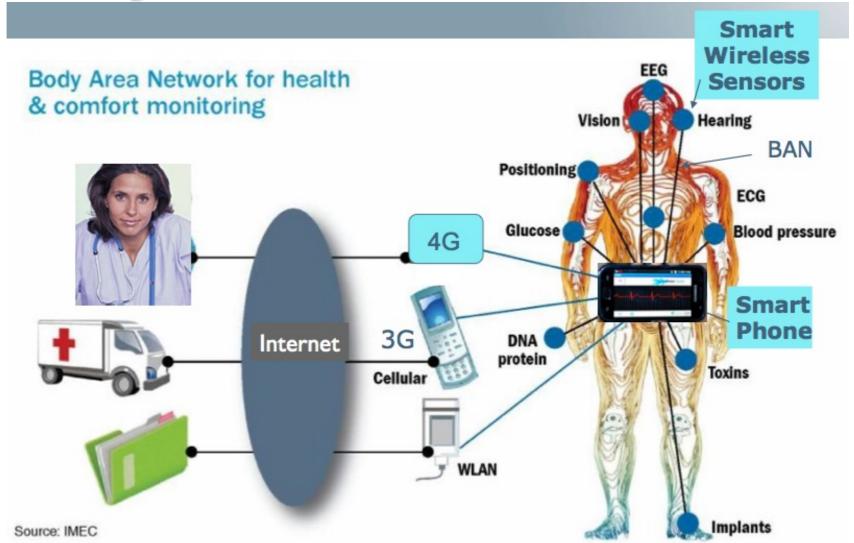
Relative Market Size by Wearable Sensor Type in 2020





Market analysis report that there will be 3 billion wearable sensors by 2025, with an overall market size of about US\$70 billion

Fully-Connected Human++



Courtesy, Hugo De Man (IMEC)

Toward innovative systems we need:

- 1. Fully integration of Biomolecules to assure specificity
- 2. Fully integration of Nano structures to assure sensitivity
- Proper CMOS frontends to assure

Bio/CMOS

and Co-Design

- (i) Precise Current measurements,
- (ii) Multiplexing for multi-metabolites,
- (iii) Reliability in Temperature and pH

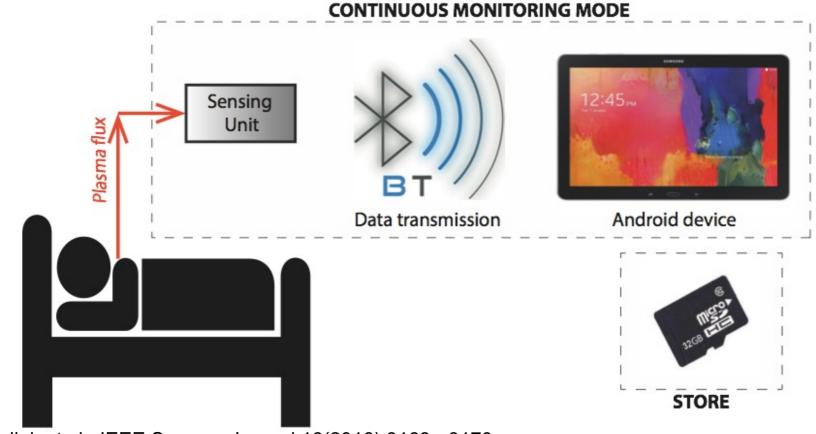
Bio/Nano/CMOS Co-design!

Portable, Implantable, 'n' Wearable



Monitoring scenarios

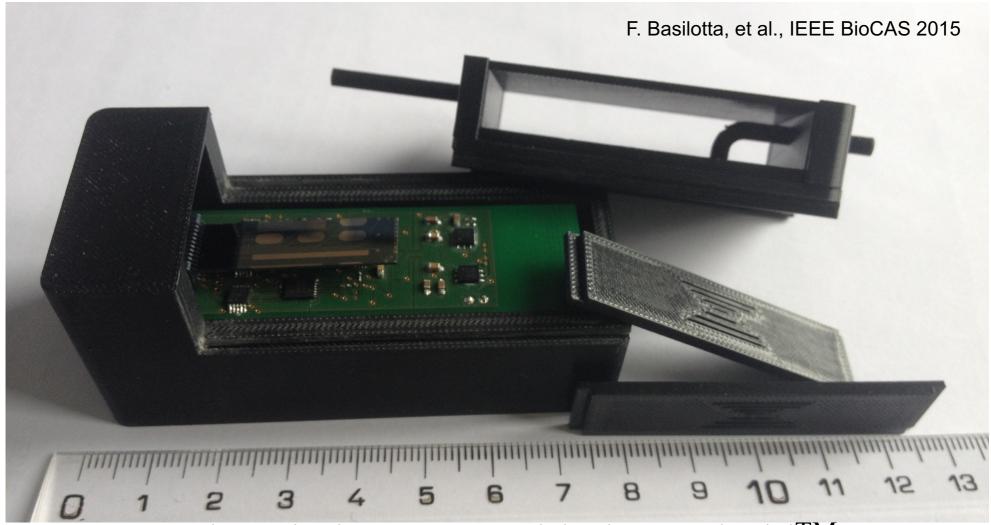
Portable: e.g., Intensive Care Units



F. Stradolini, et al., IEEE Sensors Journal 16(2016) 3163 - 3170

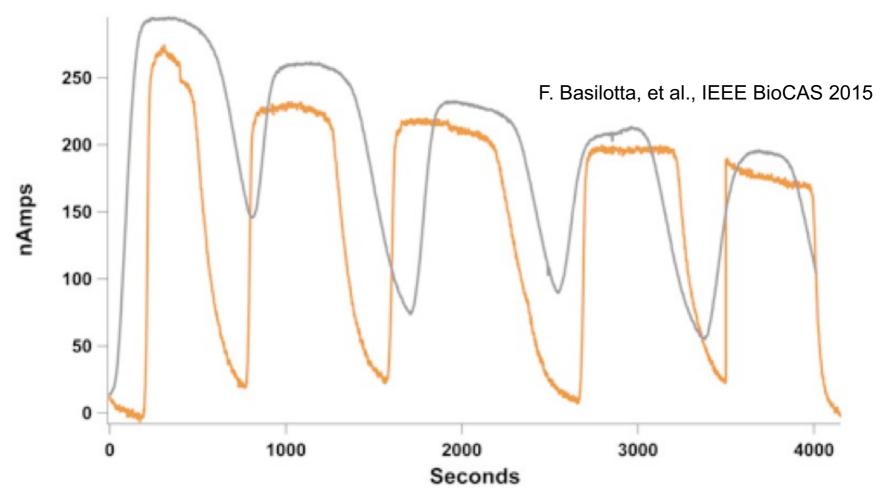
Monitoring scenario where the main parameters of the patient are continuously displayed on an Android mobile device

Monitoring in Intensive Care Units



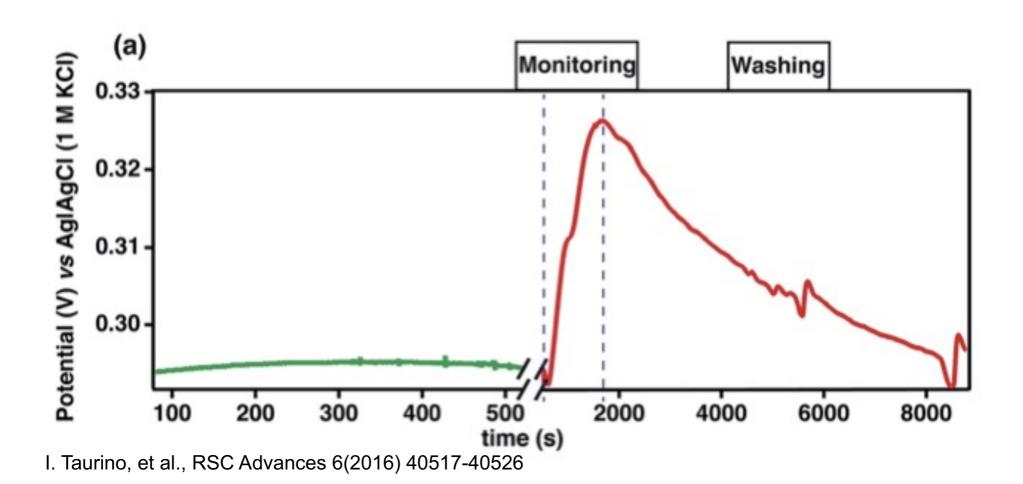
The whole system with the AndroidTM interface that allows connectivity too

Glucose and Lactate in flux



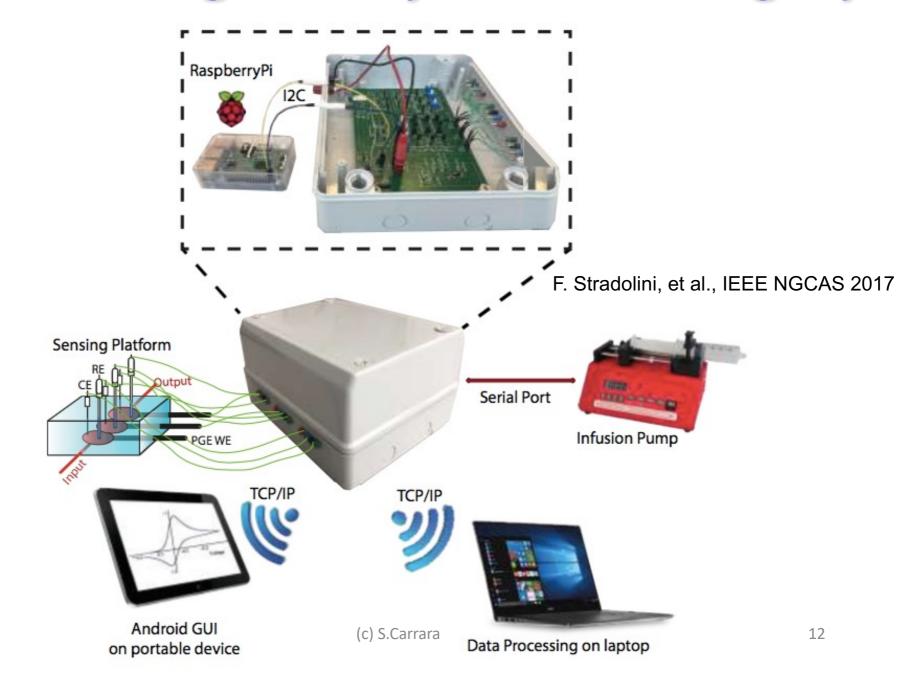
Chronoamperometry for glucose (grey) and lactate (orange) acquired with the fluidic system

Emulation of Organs Failure

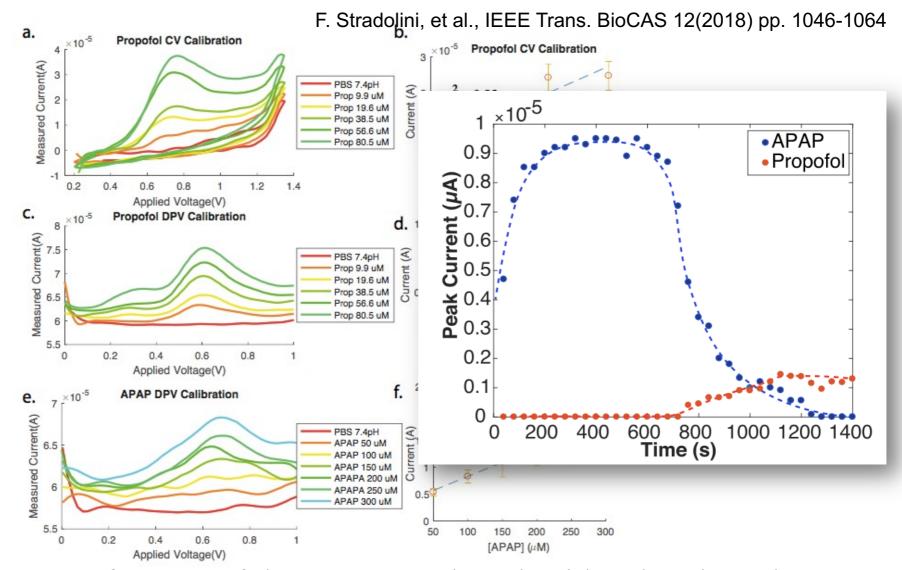


K⁺ acquisitions during cell' osmotic chock

Monitoring and Injection in Surgery

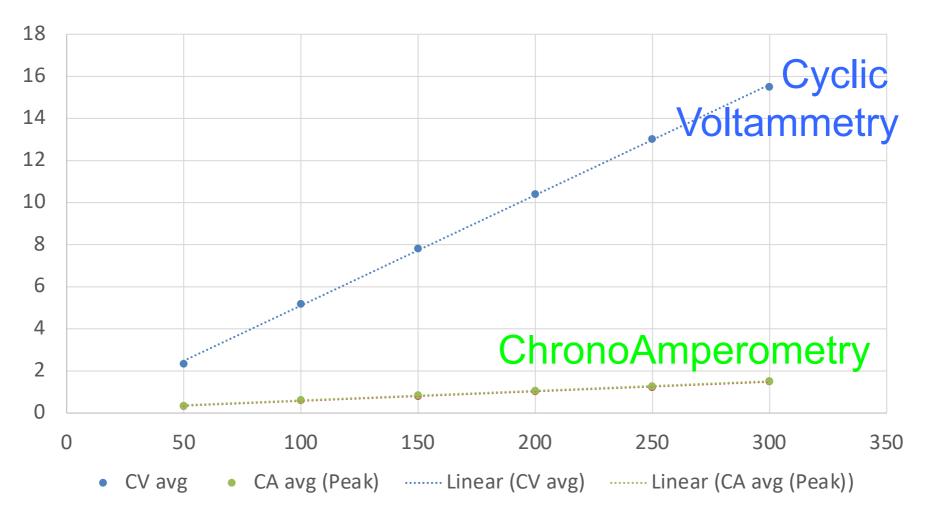


Detection of Anaesthetics



Sensors for Propofol, Paracetamol, and Midazolam have been successfully developed and tested

Chrono vs Cyclic: which best?



Paracetamol detection in Chronoamperometry or in Cyclic Voltammetry

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Lab vs Field: what change?

Stirring vs Non-Stirring

Usually, all the papers about electrochemistry we find in literature are showing data acquired with a Stirrer that assure best conditions with respect diffusion phenomena.

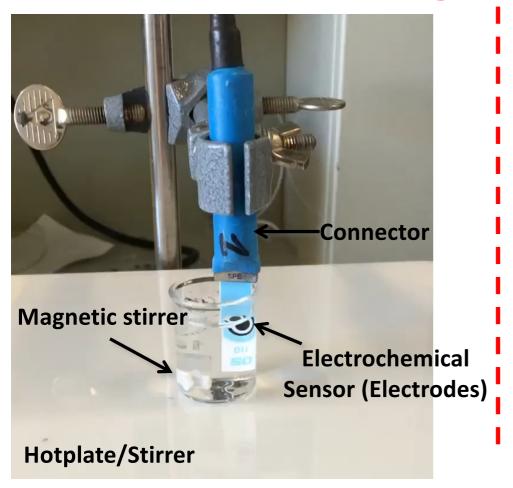
Does any conclusion we read on those papers be applied, for example, to measure on-the-skin?

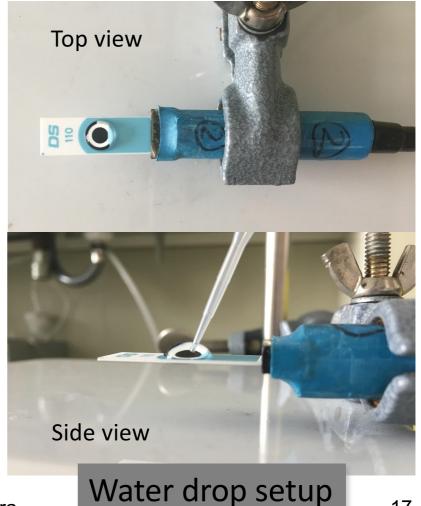
The Stirrer



Reality vs Ideality

Stirring vs non-Stirring



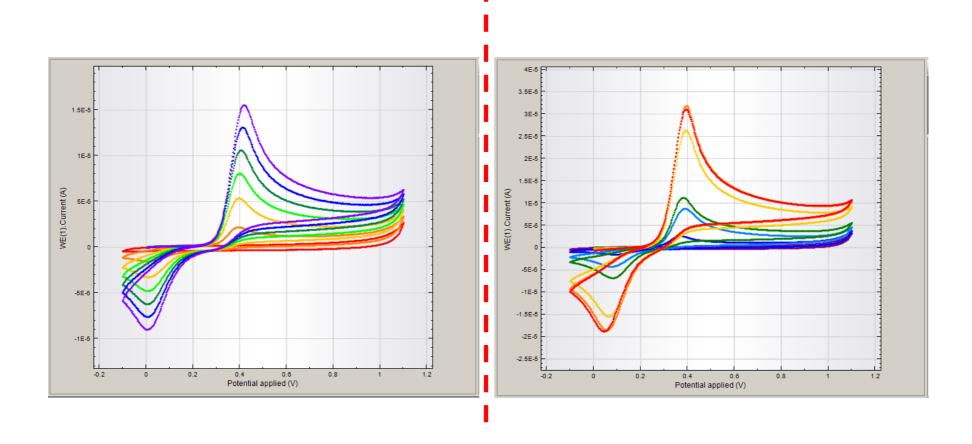


(c) S.Carrara

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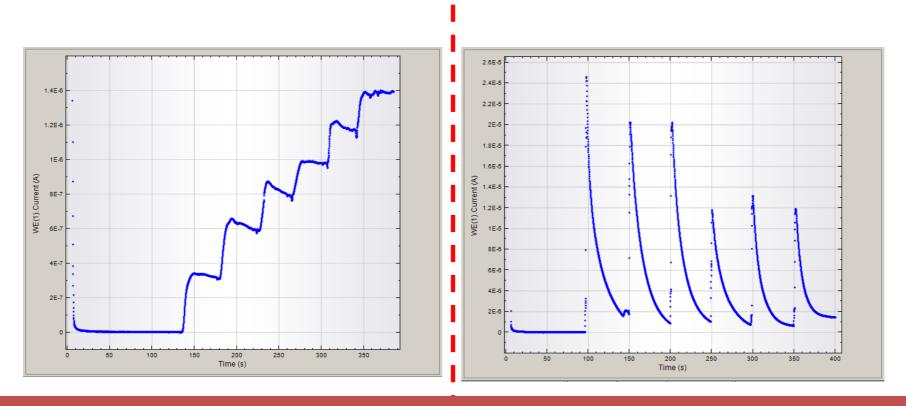
Cyclic Voltammetry

Stirring vs non-Stirring



Chronoamperometry

Stirring vs non-Stirring



APAP 0-300 uM at 0.4V, acquisition each 50 sec. in both the cases

CV vs CA

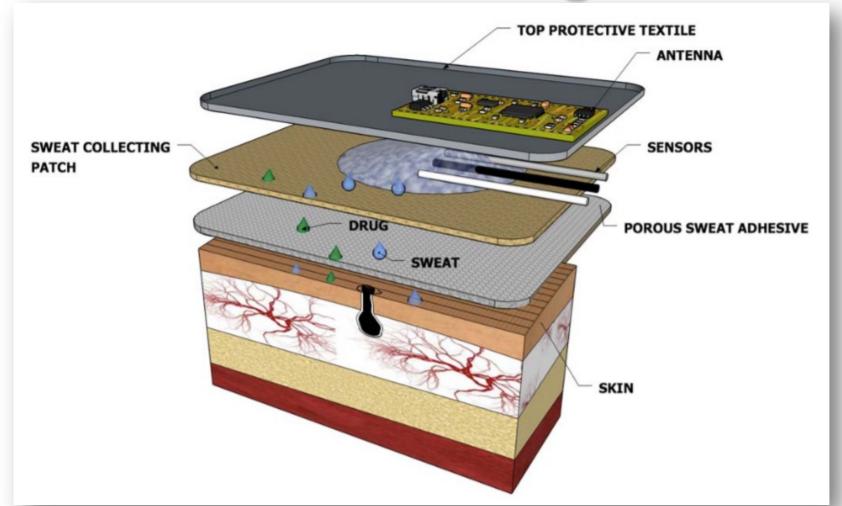
Stirring vs non-Stirring

	Stirring	Water drop
Sensitivity in CV	2.62	0.13
Sensitivity in CA	0.0045	0.012
Overall SD	low	high

In CV, both sensitivity and standard division in normal experiment are better than water drop. Therefore, the *limitation of detection of water drop experiment is* worst (higher) than normal experiment.

In CA, result is almost the same as CV but sensitivity is higher in water drop experiment. Maybe because of the injection position.

Wearable Monitoring Devices



T.Kilic, al. et S.Carrara / ICECS 2016

Metabolites Monitoring on the skin

Metabolites on the skin

I.Ny Hanitra, et al., IEEE MeMeA 2018

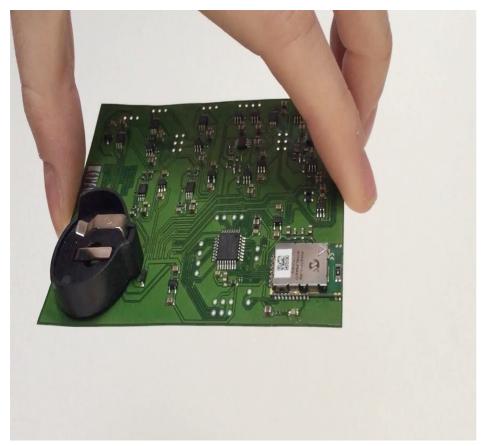
Wearable Sensors





Wearable Electronics

Flexible Electronics



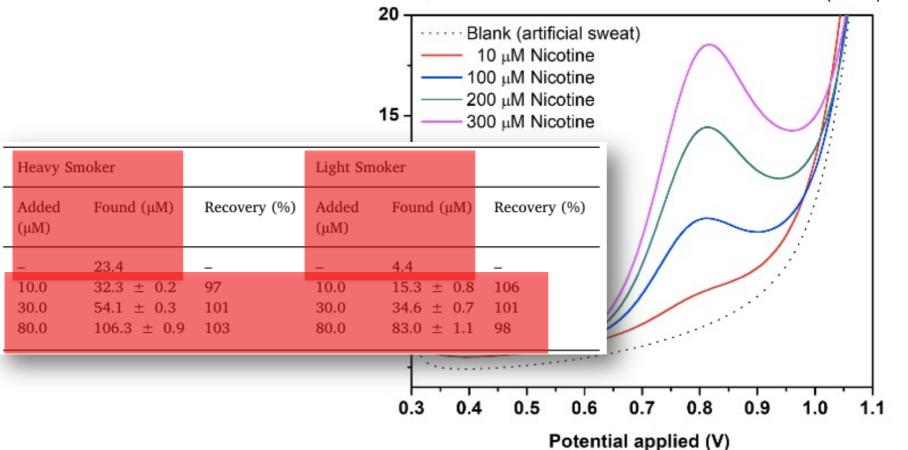
I.Ny Hanitra, et al., IEEE MeMeA 2018



The Detection system has been realized on flexible PCB

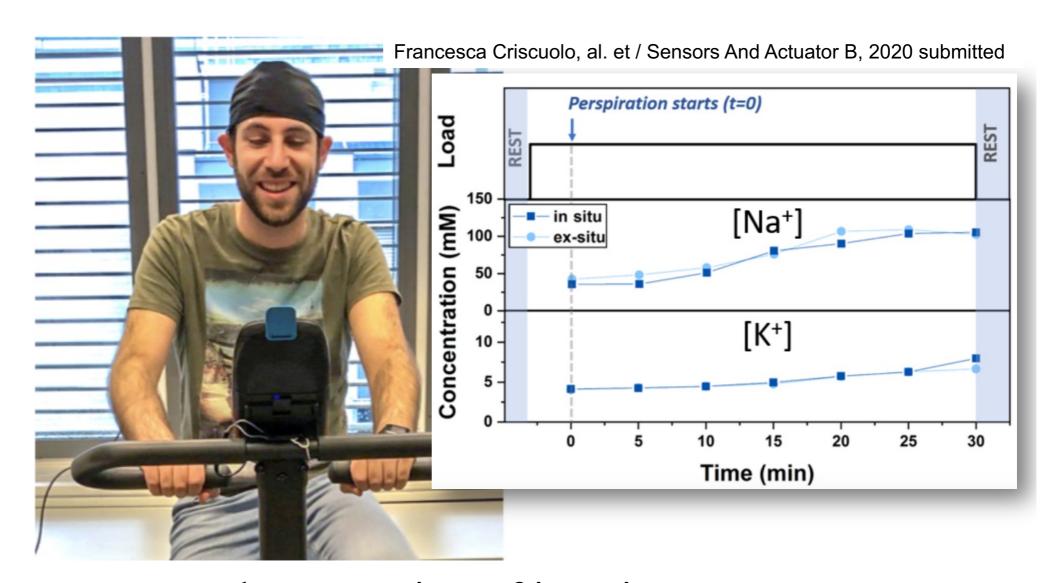
Nicotine @ Wearable





The Detection of Nicotine on the skin of heavy and light smokers

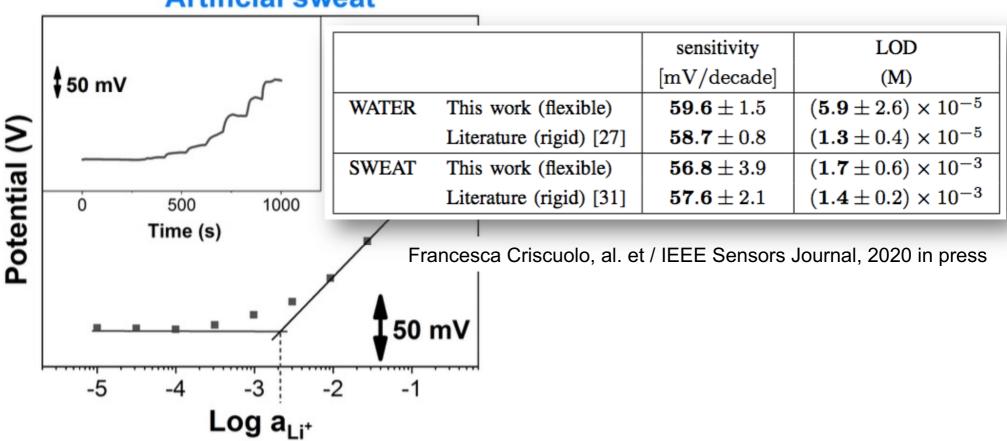
Na⁺ & K⁺ @ Wearable



The Detection of ions in sportsmen

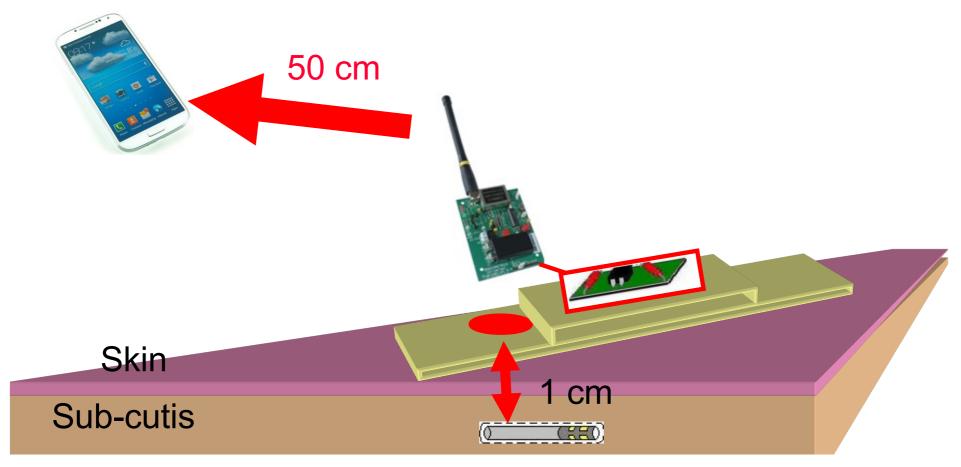
Li⁺ @ Wearable





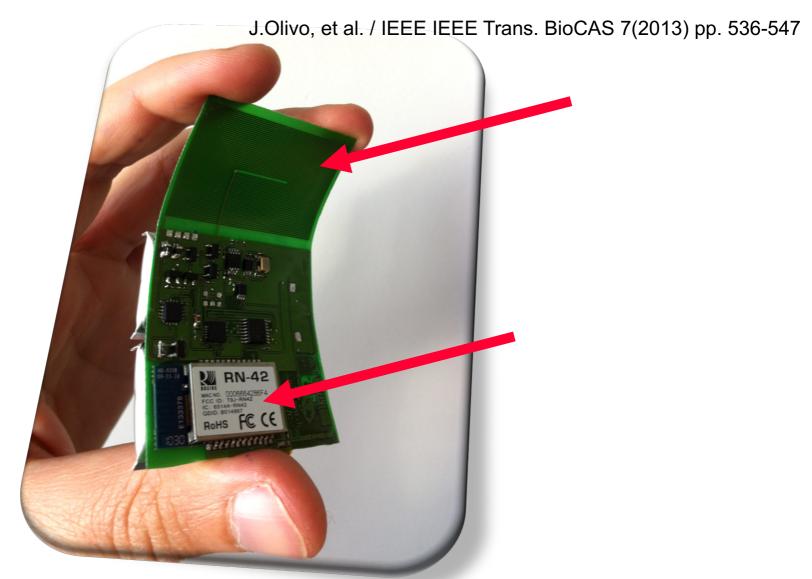
Non-invasive monitoring of Lithium as Drug in Bipolar Disorder

Under-the-Skin Devices & Wearable



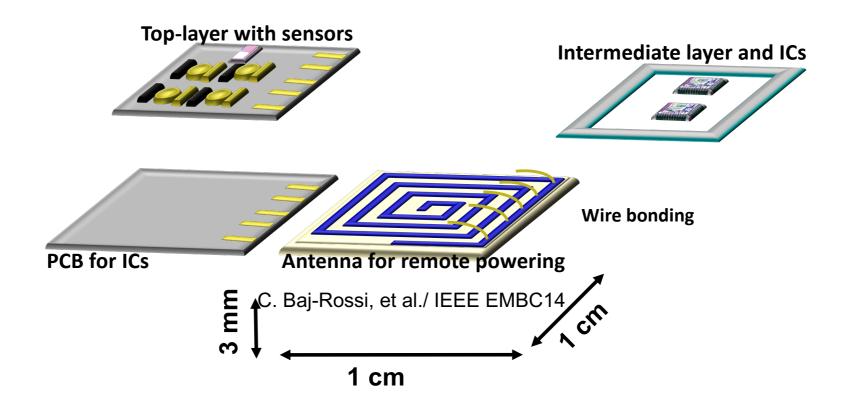
An antenna very close to the chip is required for the remote powering

The Realized Remote Powering Patch



The patch has been realized with off-the-shelf components

Under-the-Skin Device: button' size





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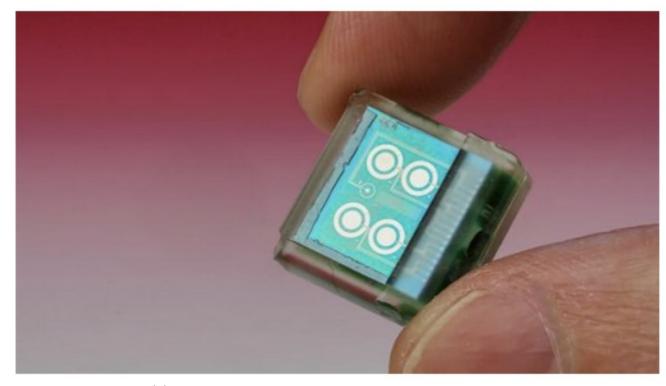
Trending News Charleston shooting Brookfield Zoo Multiple Scierosis Joe Biden

A subcutaneous biosensor chip to revolutionize tomorrow's medicine

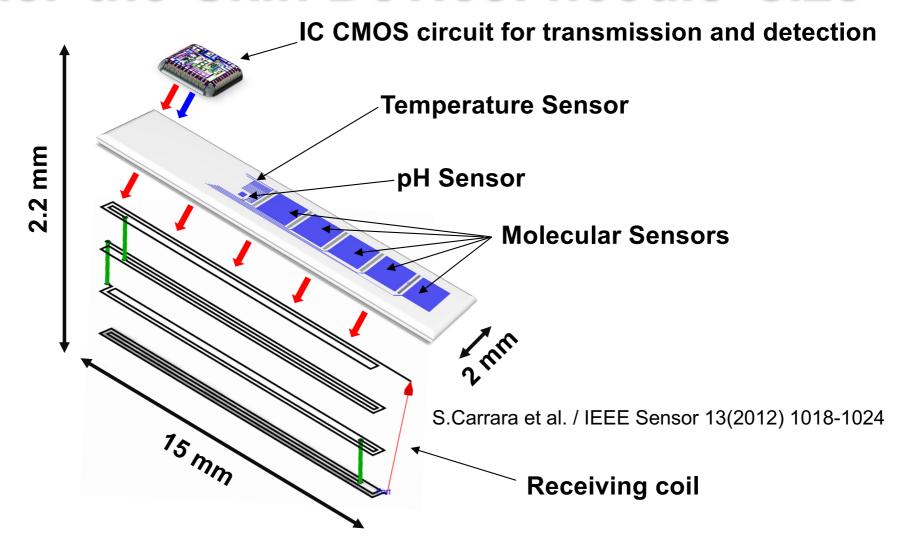
May 29, 2015 9:26 AM Relaxnews







Under-the-Skin Device: needle' size



Minimally invasive with size within that of a surgery needle

Injectable with biocompatible packaging



20 March 2013 Last updated at 01:49 GMT



'Under the skin' blood-testing device developed

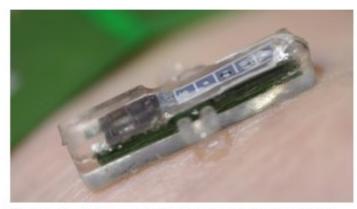
By Michelle Roberts

Health editor, BBC News online

Scientists say they have developed a tiny blood-testing device that sits under the skin and gives instant results via a mobile phone.

The Swiss team say the wireless prototype - half an inch (14mm) long - can simultaneously check for up to five different substances in the blood.

The data is sent to the doctor using radiowaves and Bluetooth technology.



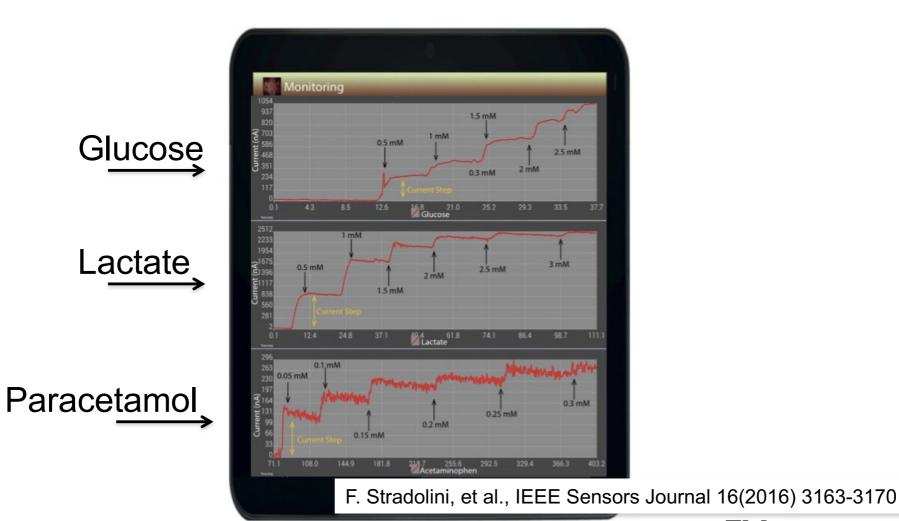
The device sits under the skin and takes multiple readings

Syringe-injectable electronics: Reveal LINQTM



Mark Phelps by Medtronic, and the Reveal LINQTM system

Android Users Interface



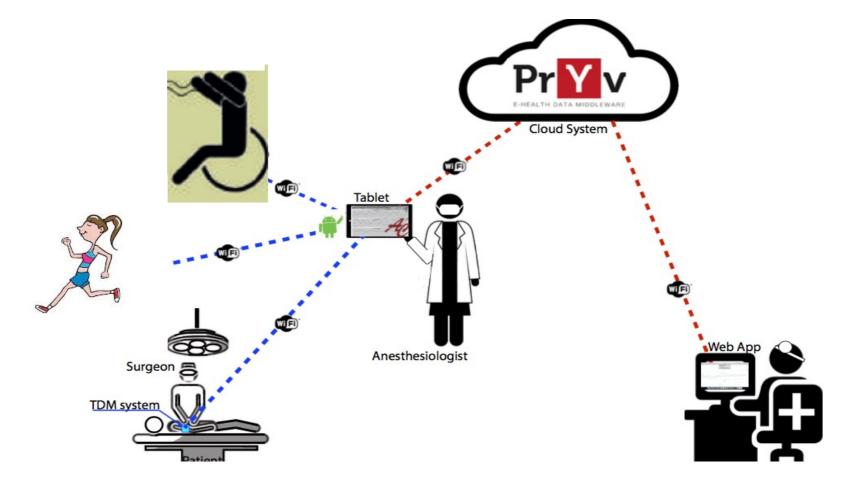
The whole system with the AndroidTM interface that allows connectivity too

Connectivity with Smart-Watch



Connectivity till the smart-watch by the WiFi network has been successfully investigated as well

Connectivity by through the Cloud



N.Tamburrano, et al., IEEE ISCAS 2018, invited paper

Connectivity by through the cloud has been successfully investigated too

Portable, Implantable, 'n' Wearable!



Monitoring scenarios

Beyond Implantable and Wearable Devices: Body Dust

Body Dust: Drinkable Electronics



Monitoring scenarios

Hyper Curve with Smart Dust



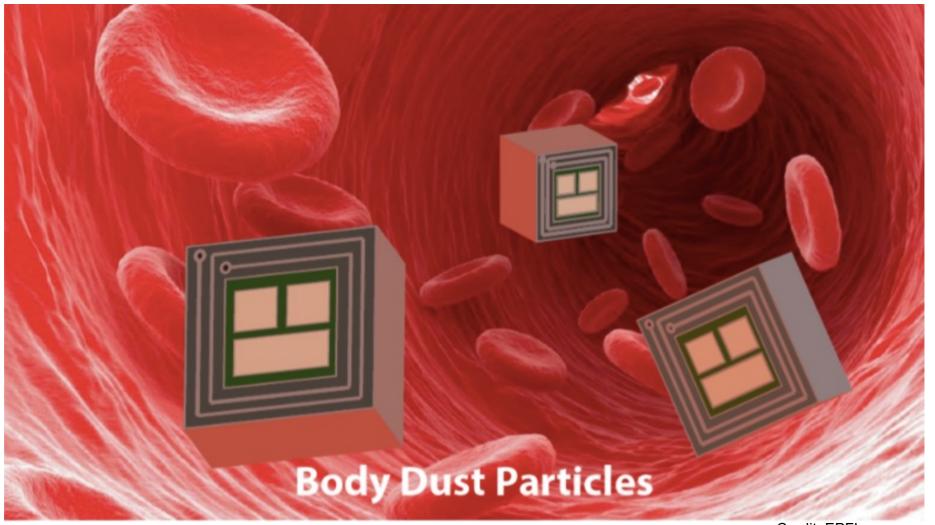
According to Gartner, "Smart dust" is set to take the technology industry by storm in the next decade [https://www.gartner.com]

The innovative concept of BODY DUST



Imagine to drink a water that contain an electronic Dust that spread in your body and then provide diagnostics

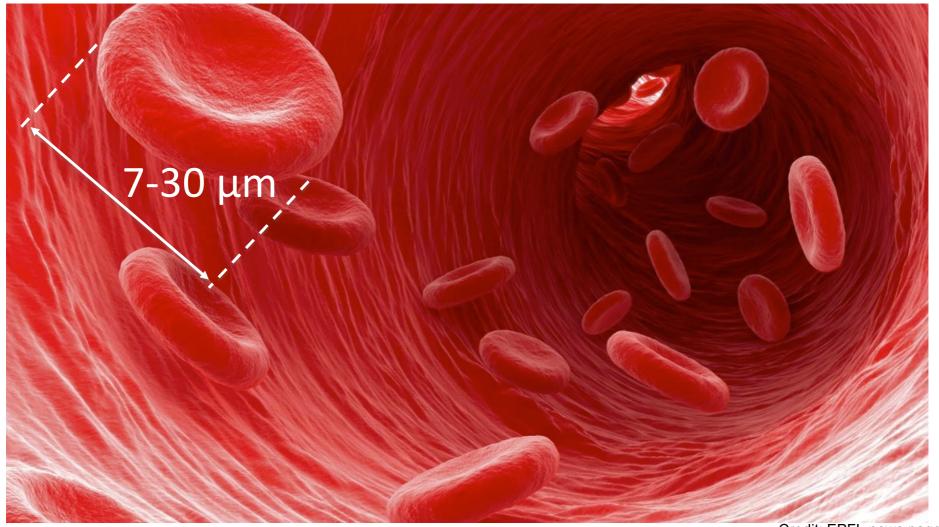
Body Dust



Credit: EPFL news pages

Tracking cancer-cell development with "drinkable" electronic sensors

Body Dust: Dramatically Small



Credit: EPFL news pages

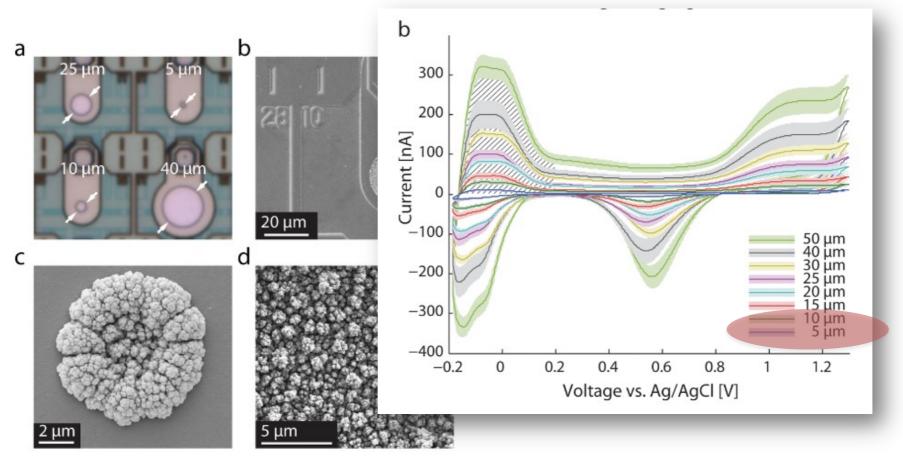
Drinkable electronics so small to be filtrated by liver and kidneys means sizes on the scale of a blood cell

Body Dust: Challenges to address!

Sandro Carrara / IEEE Sensors Journal, 2021

- (i) Extremely small sensors;
- (ii) Extremely small and thin CMOS;
- (iii) Extremely small data-link;
- (iv) Powering approaches with extremely small power-receivers;
- (v) Demonstrating in-body applications by drinking

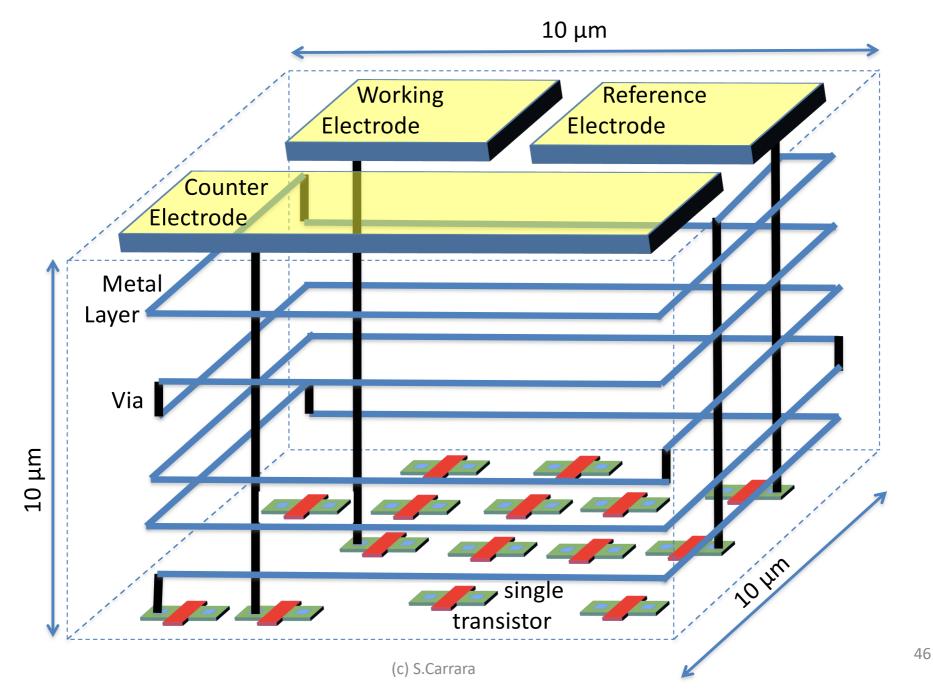
(i) Extremely small sensors;



Rothe, Joerg, et al. / Analytical chemistry 86.13 (2014): 6425-6432.

Imagine to drink a water that contain an electronic Dust that spread in your body and then provide diagnostics

(ii) Extremely small and thin CMOS;



(ii) Extremely small and thin CMOS; CMOS 0.18 μm within 10² μm^2 possible?

CMOS Body Dust - Towards Drinkable Diagnostics

Jan Snoeijs¹, Pantelis Georgiou² and Sandro Carrara¹

IEEE BioCAS 2017

Biosensor

Regulator

¹ EPFL, Lausanne, Switzeland ²Centre for Bio-Inspired Technology, Imperial College London, UK. Email: sandro.carrara@epfl.ch

AC/DC rectifier

Abstract—In this paper we introduce the concept of CMOS Body Dust. Body dust, as we envisage is to be, is a swarm of physical micro-sensing systems designed in CMOS as a cube with the size of red blood cells such

that they will be drink to deliver vital diagnos the source of a disease therefore to discuss at CMOS architecture w

total size of less than !

Keywords—Diagnostics,

factor, to be in the sar have a diameter of ar TABLE IV. TOTAL AREA AND POWER CONSUMPTION TRADE-OFF

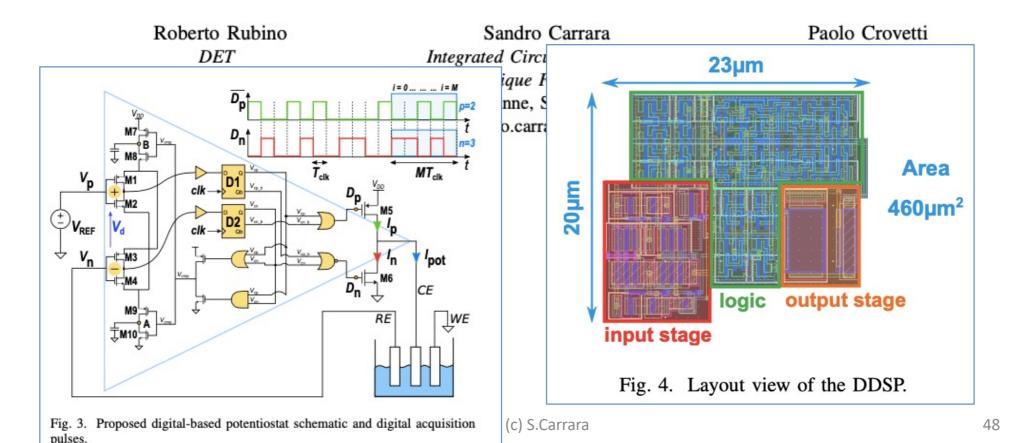
	Area [μm ²]	Power	Power [µW]	Area
	(best case)	[µW]	(best case)	$[\mu m^2]$
Potentiostat	8.7	0.141	0.124	12
I to f conv.	22	0.836	0.836	22
Rectifier	28.44	9.655	9.655	28.44
Voltage regulator	15.9	18.170	5.7	_ 24
Band-gap ref.	15.2	V 9	0.020	15.2
Pulse generator	10			10
Total	100.24	2 741		1 11.64

(c) S.Carrara 47

Band-gap

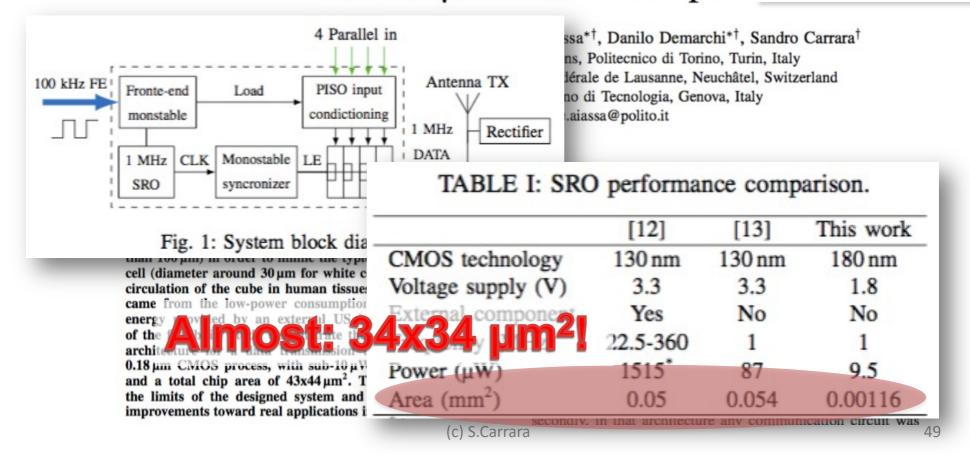
(ii) Extremely small and thin CMOS; CMOS 0.18 μm within 10² μm^2 possible?

Direct Digital Sensing Potentiostat targeting Body-Dust | EEE BioCAS 2022



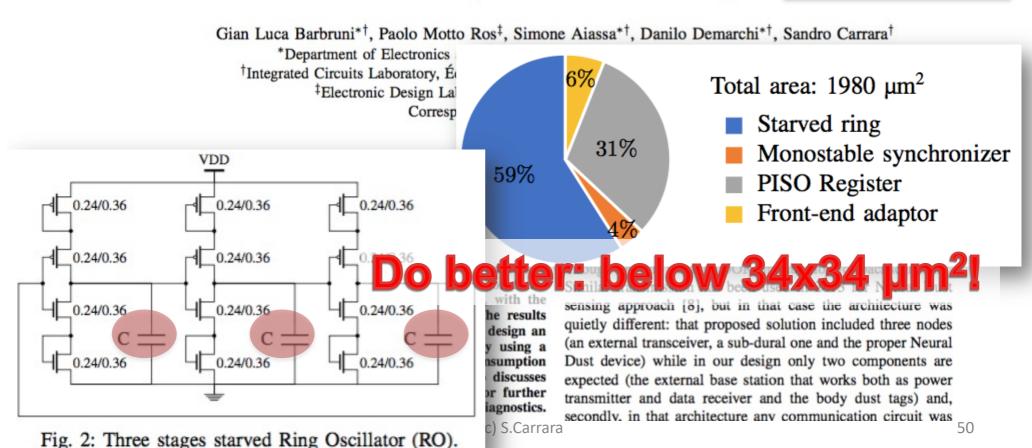
(ii) Extremely small and thin CMOS; DATA 0.18 μm transmission within 10² μm^2 ?

Body Dust: Ultra-Low Power OOK Modulation
Circuit for Wireless Data Transmission in Drinkable
sub-100µm-sized Biochips
ArXiv, December 2019



(ii) Extremely small and thin CMOS; DATA 0.18 μm transmission within 10² μm^2 ?

Body Dust: Ultra-Low Power OOK Modulation Circuit for Wireless Data Transmission in Drinkable sub-100µm-sized Biochips ArXiv, December 2019



(ii) Extremely small and thin CMOS; DATA 28 nm transmission within 10² μm²?

From 0.18 µm to 28nm Scaling CMOS Technologies for Data Links in Body Dust Applications

IEEE SENSORS 2021

Gian Luca Barbruni^{†*‡}, Paolo Motto Ros,

Danilo Demarchi* and Sandro Carrara†

†Integrated Circuits Laboratory, École Polytechnique Fédérale de Lausanne, Neuchâtel, Switzerland *Department of Electronics and Telecommunications, Politecnico di Torino, Turin, Italy

(c) S.Carrara

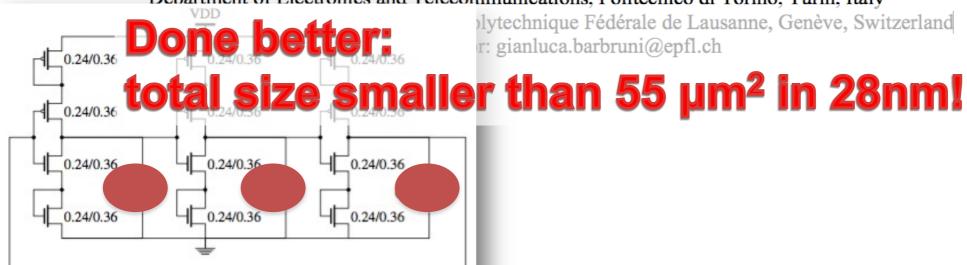
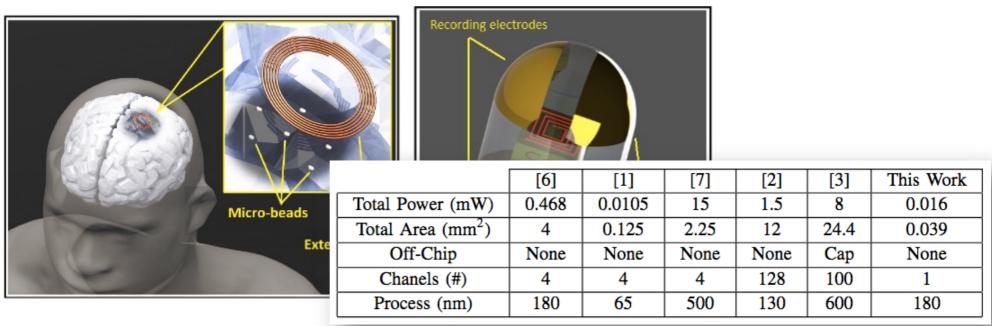


Fig. 2: Three stages starved Ring Oscillator (RO).

51

(iv) Powering approaches with extremely small power-receivers;

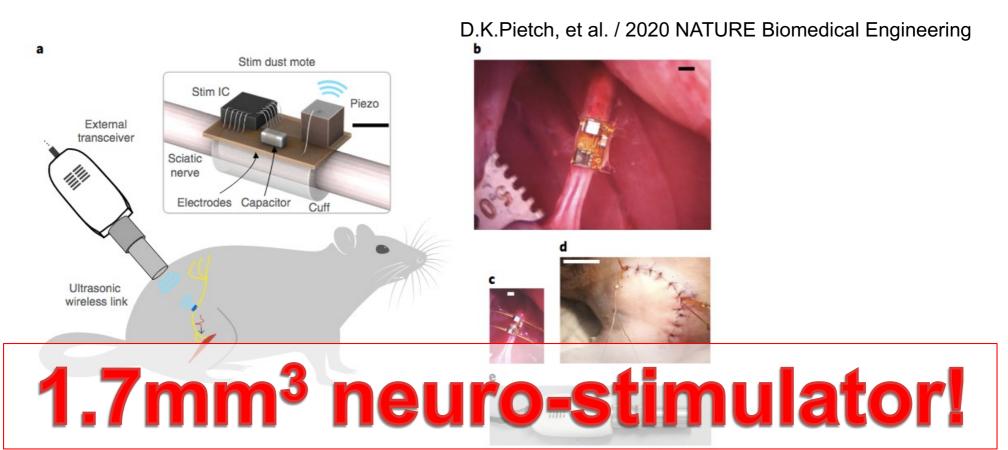
Khalifa, A., Zhang, et al. / 2016 IEEE ISCAS



200μm x 200μm coil!

16 μW received to a 0.039 mm² area-coil by inductive-link

(iv) Powering approaches with extremely small power-receivers;



65 μW received to a 1.7 mm³ volume-size transducer by ultra-sound

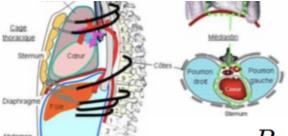
(iv) Powering approaches with extremely small power-receivers;



Three Scenarios



$$A_{min} = \frac{P_{min}}{I_d} = 1.98 \cdot 10^4 \mu m^2 \rightarrow \approx 140.81 \mu m$$



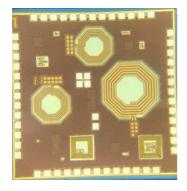
Péritoine

$$A_{min} = \frac{P_{min}}{I_d} = 4.22 \cdot 10^3 \mu m^2 \rightarrow \approx 65.6 \mu m$$

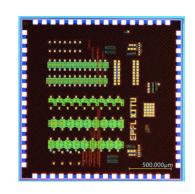
$$A_{min} = \frac{P_{min}}{I_d} = \frac{30 \cdot 10^{-6}}{1230 \frac{W}{m^2}} = 2.44 \cdot 10^4 \mu m^2 \rightarrow \approx 156 \mu m$$



Some Recent Bio/CMOS interfaces



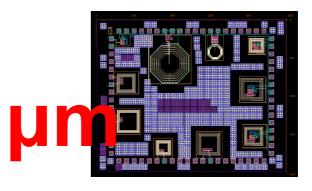
Chip # 5 TSMC 0.18 IEEE MOCAST, June 2022



Chip # 6 TSMC 0.18 (arrived October 2022)



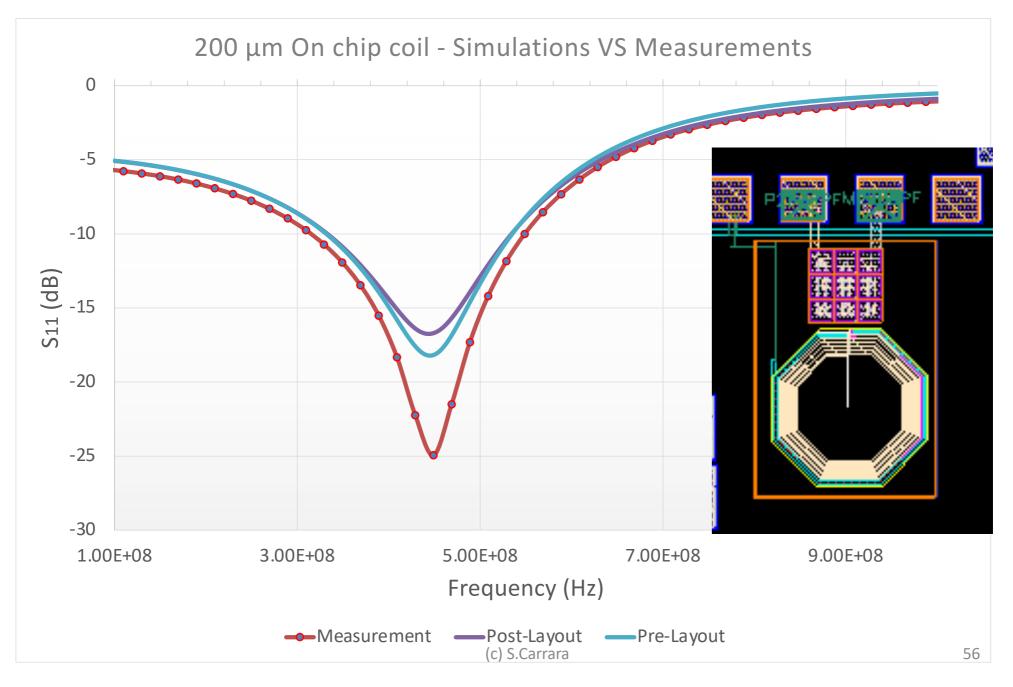
150



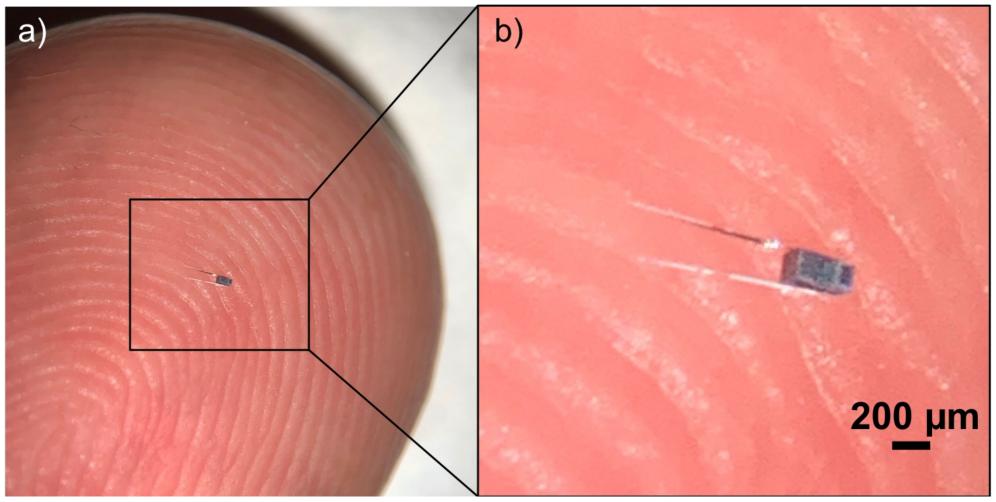
Chip # 7 TSMC 0.18 (arrived October 2022)

Chip # 8 TSMC 0.18 (Just arrived 2023)

Power Transfer to 150 um-coil



Smart Micron-sized Neural Dust



Barbruni Gian Luca, et al., PCT/IB2022/059944, 2022.

Body Dust: Challenges to address!

Sandro Carrara, al. et / IEEE Sensors Journal, 2021

- (i) Extremely small sensors;
- (ii) Extremely small and thin CMOS;
- (iii) Extremely small data-link;
- (iv) Powering approaches with extremely small power-receivers;
- (v) Demonstrating in-body applications by drinking

Conclusions

- CMOS ASICs design is still required for more reliable Bio/CMOS Interfaces and, especially, for electrochemical sensing for metabolism
- Special Biotech solutions are necessary to target the right selectivity in order to uniquely identify the right metabolic molecules
- Special Nanotech solutions are necessary to reach the right sensitivity and limit-of-detection in the ranges of concentrations on human tissues
- Automatic and continuous monitoring of the metabolism in humans is actually feasible from body tissues to our personal electronics, including portable, wearable, implantable, and may be one day also spreadable in the form of Diagnostic Dust!



EDMI Microsystems and Microelectronics

MICRO-614: Electrochemical Nano-Bio-Sensing and Bio/CMOS interfaces

Course outline

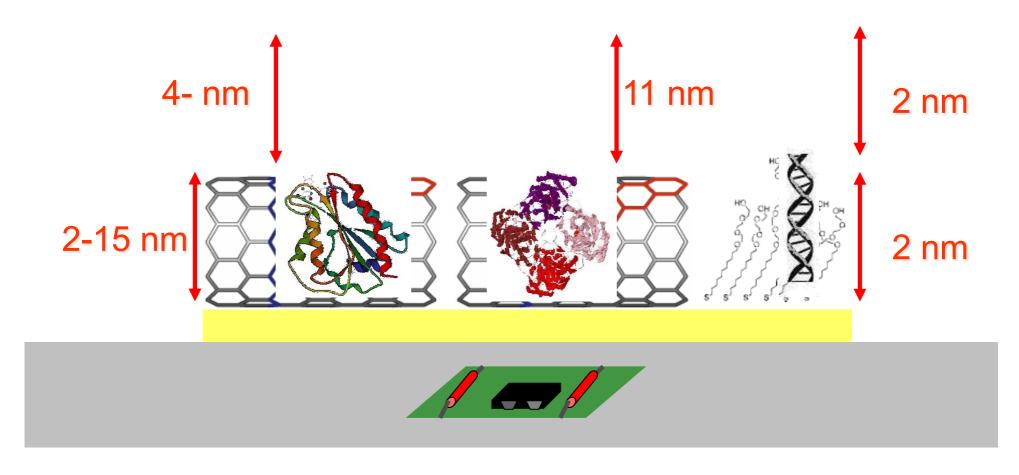
- 1. Probes and Targets Building Blocks
- 2. Probes/Target interactions (DNA & Ab)
- 3. Probes/Target interactions (Ox & P450)
- 4. Probes Detection Principles (DNA or Ox)
- 5. Probes Detection Principles (P450)
- 6. Probes immobilization
- 7. Checking Probes-layer quality (RR+SPR+SEM+AFM)
- 8. Nanotechnology to prevent Electron Transfer
- 9. Nanotechnology to enhance Electron Transfer
- 10. Nanotechnology for Memristive Biosensors
- 11. Circuits for metabolites detection in Fixed-Voltage
- 12. Circuits for metabolites detection in Scanning Voltage
- 13. Circuits for DNA Capacitance and Amperometric Detection
- 14. Circuits for metabolites detection with multi-panel systems
- 15. Summary on Bio/nano/CMOS interfaces co-design

Ummany Bio

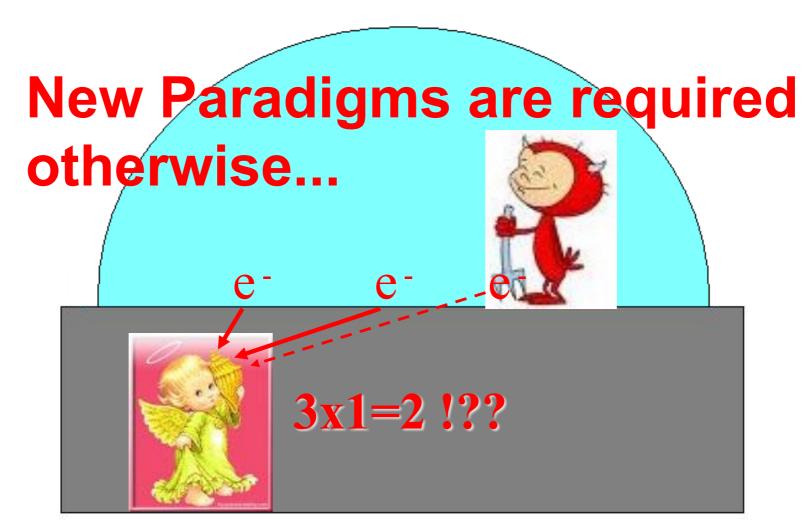
Nano

CMOS

Aim of the course

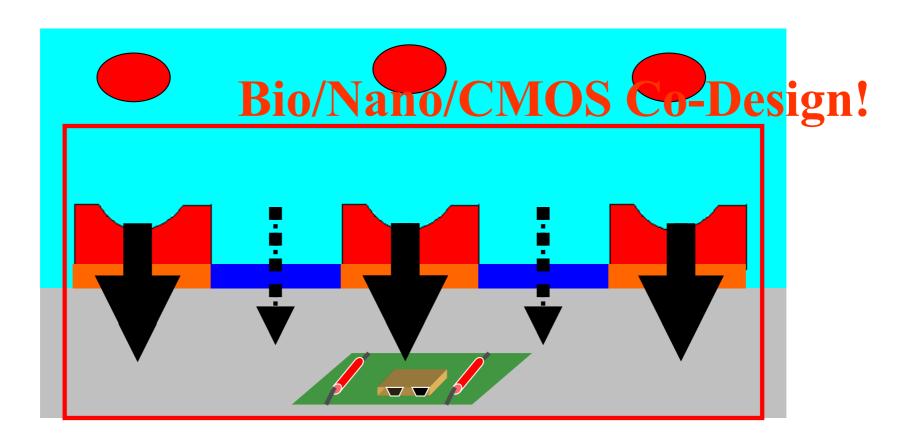


New paradigms for Nano-Bio-CMOS co-design are required to succeed in chip bio-sensing



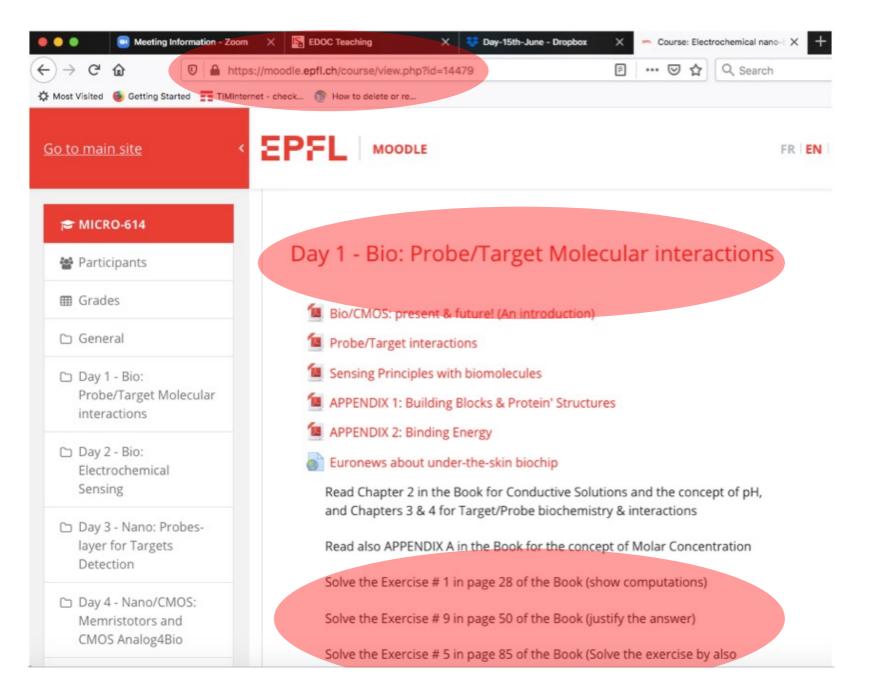
Excellent CMOS technology is not sufficient if molecules are not doing their own job at the Bio/CMOS interface!

CMOS/Sample interface



The interface between the CMOS circuit and the bio-sample needs to be deeply investigated and organized

Exercise' Solutions to get the Credit

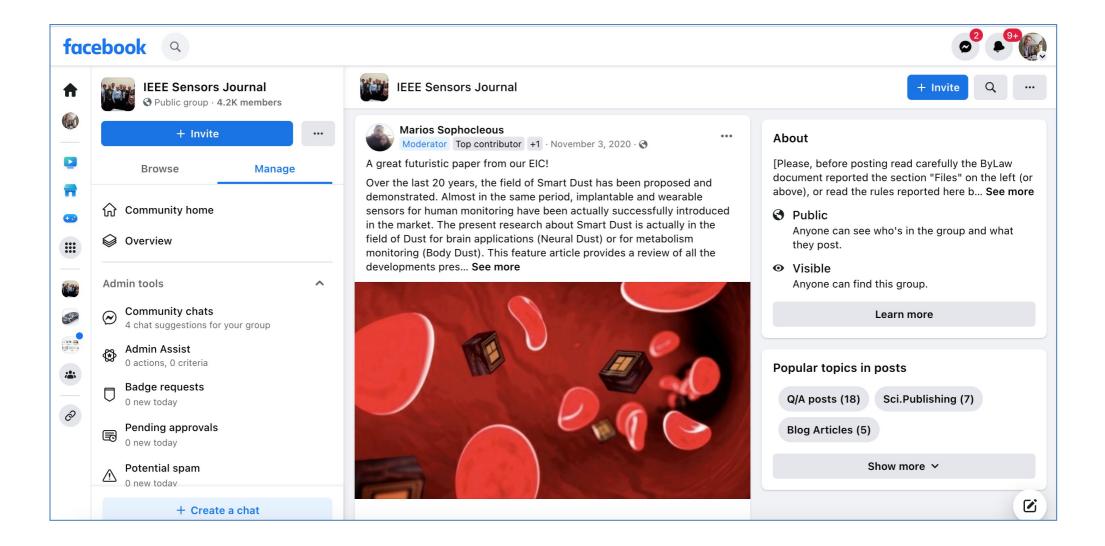


Final Work to get the Credit

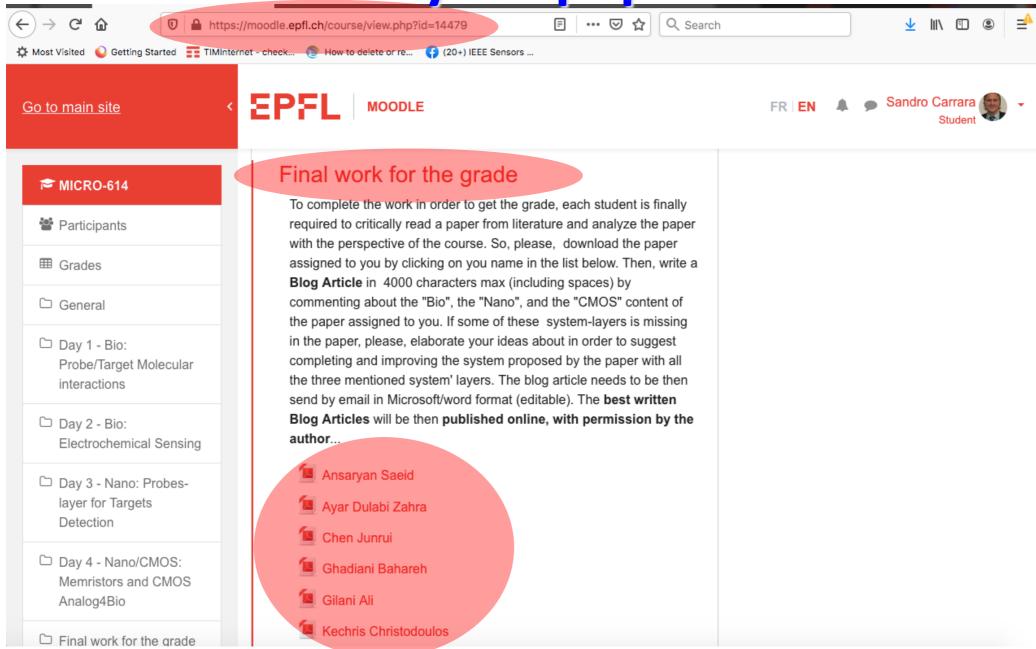
To complete the work in order to get the grade, each student is finally required to critically read a paper from literature and analyse a paper with the perspective of the course. So, please, download the paper assigned to you by clicking on you name in the list below. Then, write a **Blog Article** in 4000 characters max (including spaces) by commenting about the "Bio", the "Nano", and the "CMOS" content of the paper assigned to you. If some of these system-layers is missing in the paper, please, elaborate your ideas about in order to suggest completing and improving the system proposed by the paper with all the three mentioned system' layers. The blog article needs to be then send by email in Microsoft/word format (editable).

The best written Blog Articles will be then published online, with permission by the authors...

Media Discussion group on Sensors



Where to find your paper to discuss



Thank you to had chosen the EPFL PhD course on Electrochemical Nano-Bio-Sensing and Bio/CMOS interfaces



Coordinates

Sandro Carrara Ph.D EPFL - Swiss Federal Institute of Technology in Lausanne – Switzerland

Web: https://www.epfl.ch/labs/bci/ Email: sandro.carrara@epfl.ch

Social: https://www.facebook.com/sandro.carrara.56